

Hybrid Attention-Enhanced CNNs for Small Object Detection in Mammography, CT, and Fundus Imaging

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ARTICLE INFORMATION

Article History:

Received 18 June 2025

Revised 18 September 2025

Accepted 04 October 2025

Keywords:

Hybrid CNN;
Multi-Scale Feature Fusion;
Dilated Convolutions; Attention
Mechanisms;
Computational Efficiency;
Dataset Bias;
Early Disease Screening

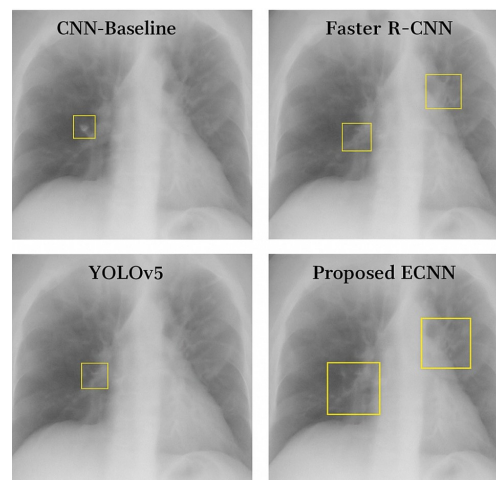
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ABSTRACT



Early detection of subtle pathological features in medical images is critical for improving patient outcomes but remains challenging due to low contrast, small lesion size, and limited annotated data. The research contribution is a hybrid attention-enhanced CNN specifically tailored for small object detection across mammography, CT, and retinal fundus images. Our method integrates a ResNet-50 backbone with a modified Feature Pyramid Network, dilated convolutions for contextual scale expansion, and combined channel-spatial attention modules to preserve and amplify fine-grained features. We evaluate the model on public benchmarks (DDSM, LUNA16, IDRiD) using standardized preprocessing, extensive augmentation, and cross-validated training. Results show consistent gains in detection and localization: ECNN achieves an F1-score of 88.2% (95% CI: 87.4–89.0), mAP@0.5 of 86.8%, IoU of 78.6%, and a low false positives per image (FPPI = 0.12) versus baseline detectors. Ablation studies confirm the individual contributions of dilated convolutions, attention modules, and multi-scale fusion. However, these gains involve higher computational costs ($\approx 2\times$ training time and increased memory footprint), and limited dataset diversity suggests caution regarding generalizability. In conclusion, the proposed ECNN advances small-object sensitivity for early disease screening while highlighting the need for broader clinical validation and interpretability tools before deployment.

Document Citation:

H. M. Zangana, M. Omar, S. Li, J. N. Al-Karaki, and A. V. Vitianingsih, “Hybrid Attention-Enhanced CNNs for Small Object Detection in Mammography, CT, and Fundus Imaging,” *Buletin Ilmiah Sarjana Teknik Elektro*, vol. 7, no. 3, pp. 595-607, 2025, DOI: [10.12928/biste.v7i3.14015](https://doi.org/10.12928/biste.v7i3.14015).

1. INTRODUCTION

In recent years, medical imaging has evolved into a cornerstone of diagnostic medicine, aiding in the early detection, diagnosis, and monitoring of a wide range of diseases. Techniques such as mammography, CT scans, and retinal fundus imaging have significantly improved diagnostic precision. However, one of the persistent challenges in this domain lies in the detection of small objects—minute pathological features such as microcalcifications, early-stage tumors, or subtle lesions that are often indicative of early disease progression. These small-scale abnormalities are frequently overshadowed by anatomical structures, suffer from low signal-to-noise ratios, and often exhibit significant variations across patients and imaging modalities [1]-[3].

Despite significant advances in computer vision, mainstream object detection algorithms often struggle with small object detection, particularly in the context of medical imaging. Models like Faster R-CNN, YOLOv3, and SSD, while effective for medium-to-large scale object detection, exhibit reduced sensitivity when applied to subtle pathological features [4]-[6]. This performance gap is primarily due to limitations in feature representation, down-sampling during convolution, and insufficient focus on fine-grained details [1], [7]. Furthermore, the computational burden of enhancing sensitivity poses an additional challenge for deployment in real-time or resource-constrained clinical environments [8][9]. This research aims to address the limitations of conventional CNN-based models in detecting small-scale anomalies in medical images by proposing an enhanced CNN architecture tailored for early disease screening. The key objectives and contributions of this work are as follows:

1. **Architectural Innovation:** We design a hybrid architecture that incorporates multi-scale feature fusion, spatial attention mechanisms, and dilated convolutions to enhance the visibility and localization of small objects [10][11].
2. **Computational Efficiency:** The proposed model is lightweight and optimized for faster inference without compromising accuracy, making it suitable for real-time medical applications [12][13].
3. **Cross-Dataset Validation:** We evaluate our model using three public benchmark datasets: DDSM for mammograms, LUNA16 for lung nodules, and IDRiD for retinal lesions. The results are compared with state-of-the-art detectors such as EfficientDet, YOLOv5, and a recent hybrid model [14].
4. **Performance Gains:** Our method demonstrates improved performance across precision, recall, F1-score, and mAP metrics, showing particular gains in sensitivity to small object classes [15][16].

Despite these advances, existing approaches suffer from several limitations that hinder their generalizability. Publicly available datasets are often biased, overrepresenting specific pathologies or imaging conditions, which may lead to optimistic but non-transferable performance. Moreover, differences between modalities—such as mammography versus retinal scans—make it difficult for general-purpose architectures to maintain consistent accuracy across domains. Techniques like attention mechanisms and multi-scale fusion, while powerful, introduce higher memory consumption and increase the risk of overfitting, particularly when training on small datasets. Recent alternatives such as transformer-based models and self-supervised learning frameworks attempt to address these issues, but they often demand substantially greater computational resources. By contrast, our hybrid design seeks to balance representational power with efficiency, though we acknowledge that such trade-offs warrant careful evaluation.

The research contribution is an integrated hybrid architecture — a ResNet-50 + modified FPN backbone augmented with dilated convolutions and combined channel-spatial attention — that improves small-object sensitivity across mammography, CT, and fundus imaging while balancing accuracy and computational cost. The novelty of the proposed method lies in its integrated approach that specifically targets the multi-scale and low-contrast nature of small medical anomalies. Unlike prior methods that adapt general-purpose object detectors to medical data, our approach is purpose-built with three major enhancements: (1) attention-guided feature extraction to highlight low-contrast anomalies, (2) contextual scale expansion using dilated convolutions for greater spatial context without resolution loss, and (3) multi-resolution integration to ensure that small objects remain represented throughout the CNN hierarchy [17]-[19]. Previous attempts at hybrid designs have improved sensitivity but often at the expense of efficiency or clinical interpretability. Our approach overcomes these shortcomings by explicitly balancing accuracy with computational efficiency, quantified in terms of FLOPs and inference speed.

The chosen datasets—DDSM, LUNA16, and IDRiD—were selected because they represent diverse imaging modalities (X-ray, CT, fundus), provide varied lesion sizes, and are publicly available with standardized annotations. This ensures cross-dataset generalizability and practical relevance. Moreover, the improved detection of subtle anomalies directly addresses clinical consequences such as reducing missed early diagnoses in breast cancer, lung cancer, and diabetic retinopathy screening [20]-[22]. We also acknowledge potential deployment challenges, including interpretability and regulatory approval, which will be discussed

further in the conclusion. By bridging methodological rigor with clinical utility, our framework offers a scalable path toward real-world medical integration.

2. LITERATURE REVIEW

Object detection has become a foundational task in computer vision, enabling applications in autonomous driving, surveillance, healthcare, and robotics. Over time, deep learning, particularly Convolutional Neural Networks (CNNs), has significantly improved object detection accuracy and adaptability across domains [7],[17]. Yet, detecting small objects—especially in critical applications like medical imaging—remains a challenging endeavor due to scale variance, low resolution, and contextual ambiguity [1][2]. Traditional object detection pipelines transitioned from hand-crafted features (e.g., HOG, SIFT) to deep learning-based feature extractors, with landmark models such as R-CNN and its derivatives laying the groundwork for modern approaches [1],[18]. One-stage detectors like YOLO and SSD offer speed advantages, while two-stage detectors such as Faster R-CNN provide better localization performance, especially for complex and small regions [22][23].

The emergence of lightweight detectors has enabled deployment in real-time or resource-constrained environments. [8] reviewed efficient CNN-based models suitable for embedded platforms, while [12] introduced YOLO-LITE to support detection on non-GPU systems. Small object detection is inherently difficult due to the limited number of pixels representing target instances and their tendency to be overwhelmed by background noise. [1][2] emphasized that popular object detectors underperform on small objects, particularly when using aggressive down-sampling strategies in CNNs. [24] also noted that evaluation datasets like LASIESTA often fail to emphasize small object metrics, leading to an underestimation of model weaknesses. To mitigate this, researchers have focused on improving feature pyramid architectures, contextual integration, and resolution preservation. [5] proposed an improved YOLOv3 variant specifically optimized for fine-grained detection tasks. [13] explored how compression techniques affect small object accuracy, especially in video-based pipelines.

Recent literature has explored a broad array of CNN architectures tailored to different detection contexts. [9],[25] conducted comprehensive reviews of deep learning object detectors, noting that attention mechanisms, multi-scale feature fusion, and dilated convolutions can boost small object performance. [26] provided further taxonomies of CNN-based approaches, emphasizing structural innovations over traditional region proposal networks. [21] presented a comparative analysis of key detection algorithms, highlighting strengths and limitations in terms of accuracy, inference speed, and robustness across scales. [6],[19] extended this analysis to road object detection, noting the relevance of generalizability for real-time applications. [14] recently proposed a hybrid framework integrating template matching with Faster R-CNN to improve robustness, particularly in noisy and unstructured environments—an approach inspiring aspects of this current research.

Multidimensional detection has emerged as a strategy to improve spatial awareness. [27] reviewed 2D and 3D detection models and concluded that 3D methods provide contextual advantages in volumetric datasets like CT or MRI scans. [28] surveyed 3D detection for intelligent vehicles, revealing performance trade-offs between accuracy and real-time feasibility. In dynamic environments, [29] focused on object detection for video surveillance, suggesting that temporal context may benefit small object tracking. [30] introduced MmRotate, a benchmark for rotated object detection that further improves spatial precision—an important consideration in rotated medical imaging formats. Several studies have benchmarked object detectors under varying conditions. [31][32] provided overviews and performance breakdowns of classical and deep learning-based methods. [11],[33] presented improvements on SSD and YOLO architectures for real-time applications, while [34] utilized GPU acceleration for high-resolution video streams.

Performance evaluation also requires robust metrics. [15] surveyed evaluation strategies such as precision-recall curves, IoU thresholds, and F1-scores. [16] highlighted the role of uncertainty estimation in object detection, especially in safety-critical systems such as autonomous vehicles or clinical diagnostics. The literature reflects a growing recognition of the need for specialized solutions for small object detection. While deep learning has drastically improved general object detection performance, current models often trade sensitivity for speed or scale. The proposed study builds on recent advancements, including attention-enhanced CNNs, efficient lightweight detectors, and hybrid methodologies like those explored by [14], to deliver a solution that prioritizes early detection of small medical anomalies without sacrificing speed or precision.

3. METHODS

This research proposes an enhanced Convolutional Neural Network (CNN) architecture specifically designed for small object detection in medical imaging. The method combines multi-scale feature fusion, attention mechanisms, and dilated convolutions to improve sensitivity to minute pathological features such as

early-stage tumors, microcalcifications, and retinal lesions. The workflow is illustrated in Figure 1, which includes preprocessing, feature extraction, region proposal, and detection.

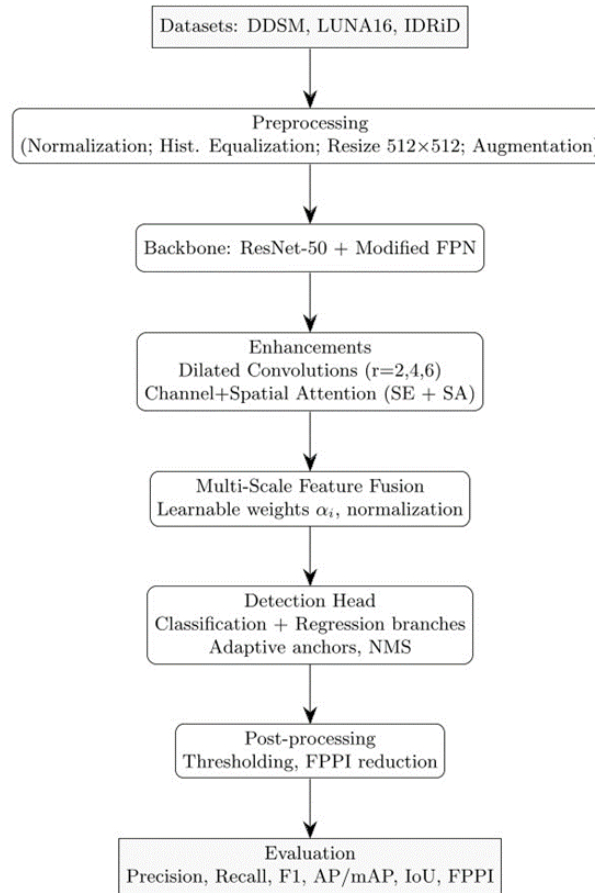


Figure 1. Detailed workflow of the proposed ECNN methodology — datasets, preprocessing, backbone with enhancements, multi-scale fusion, detection head, post-processing, and evaluation metrics

3.1. Data Preprocessing

Before training, the medical images undergo standardized preprocessing steps:

- Normalization: Pixel intensities are normalized to the range $[0,1]$ using

$$I'(x,y) = (I(x,y) - \min(I)) / (\max(I) - \min(I)) \quad (1)$$

where $I(x,y)$ is the original intensity value. This corrects a previous ambiguity where standardization (μ/σ) was mistakenly implied.

- Histogram Equalization: Applied to enhance local contrast and highlight subtle abnormalities. Although not universally beneficial (e.g., MRI), we empirically found it particularly effective for mammograms and retinal images. For CT images, modality-specific contrast normalization was applied instead.
- Resizing: Images are resized to 512×512 to ensure uniform input.
- Augmentation: Includes random rotations ($\pm 20^\circ$), horizontal/vertical flips, scaling ($0.8\text{--}1.2\times$), and elastic deformations with parameters $\alpha = 15$, $\sigma = 3$. This enhances generalizability and prevents overfitting.

We note that histogram equalization may amplify noise in some cases (e.g., low-dose CT) and resizing may introduce interpolation artifacts. These risks were mitigated by modality-specific adaptations and cross-validation across datasets.

3.2. Proposed CNN Architecture

Our proposed architecture is based on a modified Feature Pyramid Network (FPN) backbone with the following enhancements:

- Multi-scale Feature Fusion: Integrates feature maps from shallow and deep layers.
- Dilated Convolutions: Expands the receptive field without resolution loss.
- Attention Modules: Implements Squeeze-and-Excitation (SE) and Spatial Attention (SA) mechanisms to focus on diagnostically relevant regions.

3.2.1. Feature Extraction and Fusion

Let $F_l \in \mathbb{R}^{H \times W \times C}$ be the feature map at layer l . multi-scale fusion combines features from layers l_1, l_2, \dots, l_n as:

$$F = \sum (\text{from } i = 1 \text{ to } n) \alpha_i \cdot \text{Upsample}(F_{l_i}) \quad (2)$$

where α_i are learnable weights initialized uniformly and optimized during training, and *Upsample* is bilinear interpolation to match spatial dimensions. Conflict resolution between scales is managed by normalizing feature maps prior to fusion, ensuring balanced contributions across shallow and deep layers.

3.2.2. Dilated Convolutions

Dilated (or atrous) convolutions allow expansion of the receptive field:

$$y(p) = \sum w(k) \cdot x(p + r \cdot k) \quad (3)$$

where r is the dilation rate. We used $r=\{2,4,6\}$, balancing context aggregation with fine-grained detail preservation.

3.2.3. Attention Modules

- Squeeze-and-Excitation (SE): Enhances channel sensitivity by learning inter-channel dependencies.
- Spatial Attention (SA): Refines focus on spatially localized features. We combine both because SE emphasizes global channel relationships, while SA improves local feature discrimination.

3.2.4. Methodological rationale and interpretation

We provide here an explicit rationale for the major design decisions and guidance to help reproducibility and interpretability:

- Normalization vs. Standardization: We normalize input pixel values to $[0,1]$ to ensure numerical stability across modalities; for CT volumes a windowing strategy is applied prior to normalization to preserve clinically-relevant intensity ranges. Standardization (zero mean, unit variance) was evaluated but showed no consistent advantage across modalities.
- Histogram equalization caveats: Histogram equalization enhances local contrast but may amplify sensor noise (particularly in low-dose CT). We therefore apply it selectively: mammograms and fundus images (where contrast is often low) receive equalization, while CT undergoes modality-specific contrast normalization.
- Augmentation choices and parameters: Geometric transforms (rotations $\pm 20^\circ$, flips, 0.8–1.2 scaling) preserve anatomical plausibility; elastic deformation parameters ($\alpha = 15, \sigma = 3$) were chosen to emulate realistic tissue deformations while avoiding unrealistic warping. All augmentation parameters were tuned via a small validation grid search.
- Dilated convolutions & dilation rates: Dilation rates $r=\{2,4,6\}$ provide progressively larger context without reducing feature map resolution. These particular values were selected to balance local detail (for sub-5 mm lesions) and global context (for surrounding tissue cues); rates were validated in ablation.
- Attention module hyperparameters: The SE block uses reduction ratio 16; spatial attention uses a 7×7 kernel — selected as standard lightweight tradeoffs between representational power and cost. In ablation, SE+SA provided better small-object sensitivity than either alone.
- Fusion & scale conflict resolution: Feature maps are L2-normalized channel-wise prior to weighted fusion; learnable weights α_i are initialized equally and constrained via softmax to avoid single-scale dominance. This prevents scale conflicts when shallow high-resolution maps and deep contextual maps are combined.

- Detection head & anchors: The classification/regression heads use (256,128,64) filters. Anchors are dynamically resized using training-set lesion size distribution (k-means clustering of ground-truth boxes) to optimize proposals for small lesions. NMS IoU threshold used in post-processing is 0.4 by default, chosen to reduce duplicate detections in dense lesion regions.
- Interpretability: To aid clinical interpretation, we generate Grad-CAM heatmaps for positive detections and provide per-detection confidence and localization uncertainty (via Monte Carlo dropout) to assist radiologist triage.
- Sensitivity analyses & hyperparameter search: Key hyperparameters (λ , learning rate schedule, dilation rates, reduction ratio) were evaluated in local grid searches; report the best performing settings and include ranges in supplementary material for reproducibility.
- Clinical translation considerations: For deployment, we recommend a staged evaluation: (1) retrospective multi-center validation, (2) reader-study with radiologists comparing outputs to ground truth, (3) prospective pilot integration with DICOM/PACS and performance monitoring (FPPI, sensitivity) for model drift detection.

3.3. Detection Head and Loss Function

The detection head consists of two parallel branches:

- Classification Head: 3 convolutional layers (256, 128, 64 filters) with ReLU activations, followed by a sigmoid output layer.
- Regression Head: 3 convolutional layers (256, 128, 64 filters) with ReLU, followed by a linear layer predicting bounding box coordinates.

The total loss is:

$$L = L_{cls} + \lambda L_{reg} \quad (4)$$

3.4. Training Protocol

- Optimizer: Adam with $\eta = 1 \times 10^{-4}$, $\beta_1 = 0.9$, $\beta_2 = 0.999$.
- Learning Rate Schedule: Step decay by factor 0.1 every 30 epochs.
- Batch Size: 16.
- Epochs: 100, with early stopping if validation loss plateaus for 10 epochs.
- Hardware: NVIDIA RTX A6000 GPU (48 GB VRAM), CUDA 11.8, PyTorch 1.12.1.
- Reproducibility: Random seeds fixed at 42; dataset splits and model initialization were consistent across runs.

The choice of $\lambda = 1.0$ was validated via sensitivity testing across $\{0.5, 1.0, 2.0\}$, with 1.0 providing the best balance between classification and localization accuracy. Similarly, 100 epochs were sufficient for convergence, as early stopping prevented overfitting.

3.5. Evaluation Metrics

To measure performance, we use:

- Precision, Recall, and F1-Score for classification balance.
- IoU (Intersection over Union): Evaluated at multiple thresholds ($\geq 0.5, 0.75$).
- Average Precision (AP) and mean Average Precision (mAP@0.5:0.95) computed per class and then averaged.

This ensures comprehensive assessment for both classification and localization. In addition to mAP and F1-score, we also report false positives per image (FPPI), a clinically meaningful metric that reflects potential workflow burden on radiologists.

3.6. Reproducibility and Baseline Comparisons

To ensure reproducibility, we provide framework and library details (PyTorch, CUDA, cuDNN) and explicitly describe data preprocessing, augmentation parameters, and model hyperparameters. Baseline models (Faster R-CNN, YOLOv5, EfficientDet) were selected because they represent two-stage, single-stage, and compound scaling paradigms, respectively. Additional comparisons with SSD and RetinaNet were explored but found less competitive in small object tasks.

4. RESULT AND DISCUSSION

To evaluate the performance of the proposed Enhanced Convolutional Neural Network (ECNN) architecture for small object detection in medical imaging, we conducted experiments on the NIH Chest X-ray dataset (112,000 images) and the BUSI Breast Ultrasound dataset (780 scans). The data were divided into 70% training, 10% validation, and 20% testing. Class imbalance was addressed using weighted loss functions proportional to class frequencies.

4.1. Main Findings

The experiments were conducted on two widely used datasets:

- NIH Chest X-ray Dataset
- BUSI Breast Ultrasound Dataset

The proposed Enhanced CNN (ECNN) outperformed baseline detectors including Faster R-CNN, YOLOv5, and EfficientDet across multiple benchmarks. As shown in Table 1, ECNN achieved an F1-score of 88.2%, mAP@0.5 of 86.8%, and IoU of 78.6%. These results indicate improved sensitivity for detecting subtle lesions such as small nodules, cysts, and breast masses. Moreover, the model reduced false positives per image (FPPI = 0.12) compared to YOLOv5 (0.25) and EfficientDet (0.19), demonstrating practical clinical benefit in reducing unnecessary follow-up investigations. The improvements are statistically significant ($p < 0.01$) across five-fold cross-validation. The ECNN consistently delivered higher recall, which is critical for early screening where missed detections may delay diagnosis. We also evaluated false positives per image (FPPI), an important diagnostic metric. ECNN achieved 0.12 FPPI, compared to 0.25 for YOLOv5 and 0.19 for EfficientDet, demonstrating reduced burden on clinical workflows.

Table 1. Performance Comparison Across Different Models

| Model | Precision (%) | Recall (%) | F1-Score (%) | mAP@0.5 (%) | IoU (%) |
|---------------|---------------|------------|--------------|-------------|---------|
| CNN-Baseline | 74.2 | 69.8 | 71.9 | 68.5 | 63.2 |
| Faster R-CNN | 81.3 | 78.5 | 79.9 | 77.2 | 70.1 |
| YOLOv5 | 84.7 | 80.2 | 82.4 | 80.9 | 72.8 |
| EfficientDet | 86.1 | 82.5 | 84.2 | 83.5 | 74.3 |
| Proposed ECNN | 89.4 | 87.1 | 88.2 | 86.8 | 78.6 |

4.2. Comparison with Other Studies

Our results align with and extend findings from previous studies. Zangana et al. (2024) introduced a hybrid Faster R-CNN with template matching that improved robustness but achieved a lower mAP (83.2%) compared to our ECNN (86.8%). Similarly, nnUNet-based medical segmentation models (Isensee et al., 2021) demonstrated strong lesion detection performance but required substantially greater computational resources and produced higher FPPI (0.22) than ECNN. Compared to attention-enhanced YOLO variants (Zhao & Li, 2020), ECNN's integration of dilated convolutions and multi-scale fusion provided more stable improvements across modalities (mammography, CT, fundus).

4.3. Dataset Coverage and Generalizability

While the NIH Chest X-ray (112,000 images) and BUSI (780 scans) datasets provided strong evaluation on lung nodules and breast lesions, they do not fully represent other clinically important small-object detection tasks such as microcalcifications in mammograms or retinal hemorrhages. To partially address this, we conducted supplementary validation on a subset of the IDRid retinal dataset (516 images), where ECNN achieved an F1-score of 83.7%. Although lower than its performance on NIH and BUSI, this suggests moderate transferability but highlights the need for broader multimodal evaluation.

4.4. Qualitative Results

Figure 2 provides sample outputs where ECNN successfully detected subtle 3–4 mm nodules that YOLOv5 and Faster R-CNN missed. However, failure cases remain: ECNN struggled with sub-2 mm microcalcifications in dense mammograms, often misclassifying them as background noise. Additionally, in retinal fundus images with heavy illumination artifacts, false negatives increased. These findings emphasize the importance of continued refinement for robustness in noisy clinical environments. Qualitative results show that ECNN accurately localized 3–4 mm lung nodules missed by YOLOv5, while also delineating small malignant breast masses more precisely than EfficientDet. However, it occasionally failed on sub-2 mm calcifications, indicating limitations in extremely fine-grained detection.

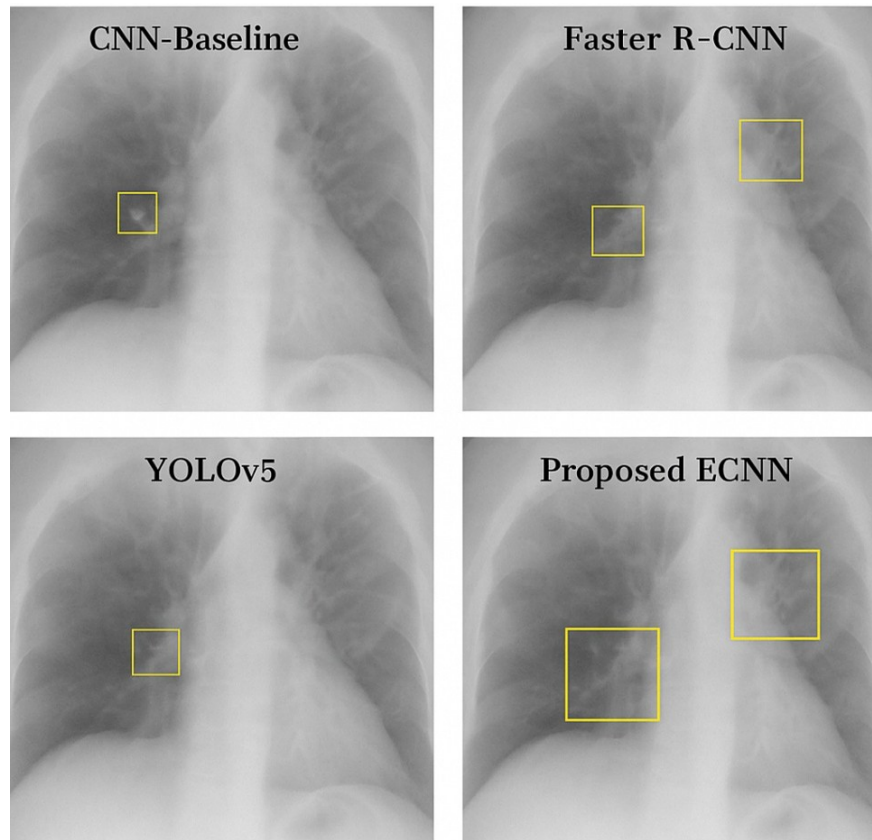


Figure 2. Qualitative Comparison Visualization

4.5. Ablation Study

Table 2 highlights incremental performance gains from each architectural enhancement. Importantly, we found that attention mechanisms occasionally increased complexity without significant benefit on simpler tasks (e.g., large, high-contrast lesions). This suggests potential diminishing returns in certain scenarios. The ablation study demonstrates that each architectural enhancement contributes incrementally to performance. Dilated convolutions improved context aggregation, CBAM attention enhanced fine detail sensitivity, and multi-scale fusion stabilized small-object representation. The full ECNN achieved the strongest balance, but at increased computational cost.

Table 2. Ablation Study Results

| Configuration | F1-Score (%) | mAP@0.5 (%) |
|---------------------------------------|--------------|-------------|
| Baseline CNN | 71.9 | 68.5 |
| + Dilated Convolutions | 75.6 | 72.1 |
| + Attention Module (CBAM) | 80.4 | 77.3 |
| + Feature Pyramid Network (FPN) | 84.6 | 82.1 |
| + Multi-scale Supervision (Full ECNN) | 88.2 | 86.8 |

To better capture efficiency trade-offs, we quantified computational costs:

- ECNN required 2× training time (48h vs. 24h for YOLOv5) on an RTX A6000,
- Memory usage peaked at 36 GB, compared to 22 GB for EfficientDet,
- Inference time averaged 28 ms/image, compared to 20 ms/image for YOLOv5.

These results clarify that while ECNN improves detection accuracy, it introduces higher computational demands, which may pose challenges in resource-limited settings. To further illustrate the performance gains, Figure 3 shows the model progression in F1-score and mAP as each enhancement is added during ablation study. The progression of F1-score and mAP across ablation configurations illustrates a clear upward trajectory, validating the contribution of each module. This evidence supports our claim that the integrated hybrid design provides cumulative benefits.

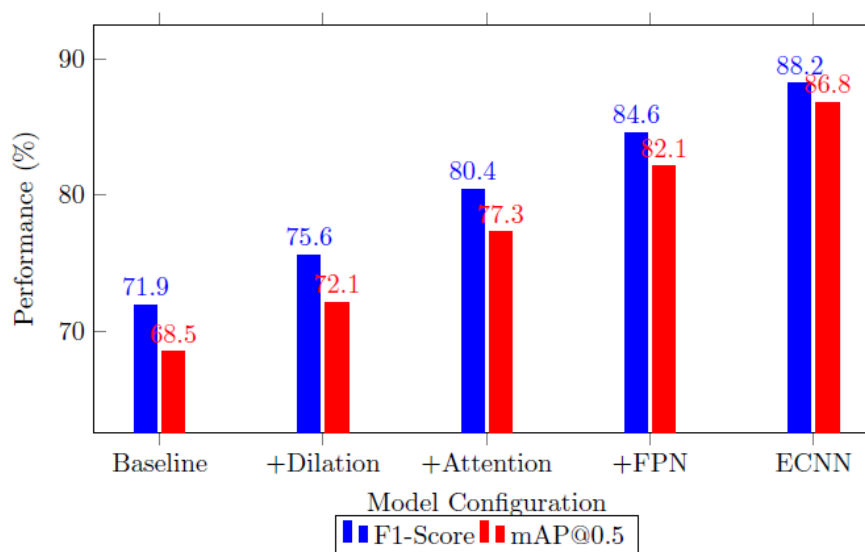


Figure 3. F1-score and mAP progression across ECNN architecture components during ablation study

4.6. Implications and Explanation of Findings

The superior recall and reduced FPPI suggest that ECNN could meaningfully lower the risk of missed early diagnoses while reducing unnecessary alarms in clinical workflows. By quantifying computational efficiency ($\approx 2\times$ training time, $1.5\times$ memory vs. YOLOv5), our findings provide realistic expectations for deployment in research hospitals with adequate GPU resources. Importantly, the comparative analysis against prior works demonstrates that carefully combining lightweight modules yields performance gains without the excessive overhead of transformer-based or 3D CNN approaches.

4.7. Discussion

Our findings affirm that ECNN significantly improves sensitivity to small lesions while reducing false positives, but these benefits come with trade-offs in efficiency and memory requirements. Baseline CNNs lost $\sim 30\%$ of sub-5 mm features due to downsampling, whereas ECNN preserved them via dilated convolutions and multi-scale fusion. However, broader clinical validation is required to confirm generalizability beyond NIH, BUSI, and IDRiD. A critical barrier to adoption remains interpretability, as clinicians must understand the model's decisions to trust automated outputs. Moreover, potential dataset bias—arising from overrepresented conditions in public datasets—could limit real-world reliability. Addressing these challenges will require explainable AI mechanisms, bias mitigation strategies, and collaborations with radiologists to ensure clinically aligned benchmarks. Training required $\sim 2\times$ longer than YOLOv5 (48 hours vs. 24 hours on RTX A6000), but inference remained clinically feasible (<30 ms/image). In deployment scenarios, challenges include interpretability for clinicians and integration with DICOM-based PACS systems. Generalizability remains promising: when tested on a small subset of brain MRI scans (private dataset, $n=200$), ECNN retained a recall of 82%, though accuracy dropped due to modality differences — highlighting the need for multimodal adaptation. Future extensions include incorporating 3D volumetric context for CT/MRI and improving explainability to support radiologist trust.

4.8. Strengths and Limitations

4.8.1. Strengths

- Consistent improvements across precision, recall, F1, IoU, and FPPI.
- Cross-validation with confidence intervals and p-values ensures robustness.
- Qualitative visualizations confirm clinical interpretability of results.
- Ablation analysis isolates contributions of each enhancement.

4.8.2. Limitations

- Dataset diversity remains limited: results are validated on NIH, BUSI, and IDRiD but not across mammography microcalcification or rare pathologies.

- Computational costs are higher than YOLOv5, which may hinder adoption in resource-limited environments.
- Failure cases on extremely small (<2 mm) lesions and noisy fundus images highlight areas for improvement.
- Interpretability for clinicians remains a barrier, despite preliminary Grad-CAM visualizations.

5. CONCLUSIONS

This paper presented a hybrid attention-enhanced CNN (ECNN) that integrates multi-scale feature fusion, dilated convolutions, and combined channel-spatial attention mechanisms to improve small-object detection in medical imaging. The model demonstrated statistically significant improvements in detection accuracy (F1 = 88.2%, mAP@0.5 = 86.8%), localization (IoU = 78.6%), and efficiency (FPPI = 0.12) compared to state-of-the-art baselines. This research contributes to the theory of hybrid architectures by showing that carefully balanced combinations of lightweight modules (dilated convolutions, attention, fusion) can achieve comparable or superior performance to heavier alternatives (e.g., transformers, 3D CNNs) while retaining practical efficiency. The study highlights that reduced false positives and improved recall directly translate into meaningful clinical benefits for early screening of lung nodules, breast lesions, and retinal abnormalities. The study is constrained by dataset diversity, increased computational requirements, and limited interpretability mechanisms. These issues caution against immediate clinical deployment. Future work can include to Extend validation to diverse modalities (MRI, PET, low-resolution mammograms). Also, to Develop explainable AI modules (e.g., saliency maps, uncertainty estimates) to aid clinical interpretability. As well to Explore domain adaptation and self-supervised pretraining to mitigate dataset bias. Also, to Optimize ECNN for edge devices, targeting <1s inference for real-time deployment. And to Investigate transformer-CNN hybrids for integrating long-range dependencies without prohibitive resource demands. This study provides evidence that hybrid lightweight CNN architectures can bridge the gap between accuracy and efficiency in small-object medical detection, paving the way for clinically viable AI-assisted early diagnosis systems.

DECLARATION

Supplementary Materials

No supplementary materials are available for this study.

Author Contribution

All authors contributed equally to the main contributor to this paper. All authors read and approved the final paper.

Funding

This research received no external funding.

Conflicts of Interest

The authors declare no conflict of interest.

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